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A Robust and Secure Medical Image Watermarking Algorithm Based on Normalized DCT and Polar-coded UFMC Assisted NOMA Scheme for Telemedicine Applications

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Abstract: This paper proposes a novel medical image watermarking scheme for a multiuser wireless system based on data normalization and polar code. The watermark image is normalized, converted into a set of coefficients using Discrete Cosine Transform (DCT), and then embedded with host medical image coefficients. The watermark image is encrypted using a Baker map and then normalized. The normalized value is converted to binary data, then XORed with a logistic map sequence, and employed as frozen bits in polar code to achieve security, robustness, and imperceptibility over the Non-Orthogonal Multiple Access-Universal Filtered Multicarrier (NOMA-UFMC) transmission scheme. A collection of medical images was employed to evaluate the proposed technique for two users, and the findings are Peak Signal to Noise Ratio (PSNR=69.5761), structural similarity index (SSIM=0.9966), mean square error (MSE=0.4399) and Normalized Cross-Correlation (NCC=0.9997) which demonstrate that it is capable of achieving a high level of imperceptibility and robustness against attacks. In addition, the proposed scheme produced good Bit Error Rate (BER) performance by exploiting the properties of polar code. Compared with the traditional techniques, the proposed approach has higher image quality, a secure watermark image, performs high robustness against various attacks, and has low execution time (about 0.3284 seconds). The suggested method is, therefore, a promising one for protecting medical images in healthcare settings.

Keywords: Watermarking, Medical images, DCT, Polar code, NOMA, UFMC.

1. Introduction

Digital existence has permeated people's lives as a result of the merge of the internet in medical devices technology. Currently, almost of medical information must be delivered over the Internet, which includes text, images, videos, and other types of media. This makes the transmitted data more vulnerable to manipulation and theft, considerably increasing the danger of patients' privacy being compromised. Thus, enhancing the security of medical data is a critical matter that must be addressed right now. The digital watermarking techniques further improve the conventional encryption techniques. It can be considered a technology for hiding information because its invisibility not only hides the patient's data but also won't influence the physician's evaluation of the host image, enhancing the safety of the patient's privacy [1]. With watermarking, specific information called a watermark is added to the host image which can later be extracted to verify its authenticity [2]. Different approaches have been devised for the secure transmission of medical images and the data that is hidden inside them. The fundamental objective is that the secret message cannot be extracted from the image by anyone but only the authorized parties. Medical image watermarking indicates the hiding of digital marks, such as the hospital's logo (name) or Electronic Patient Information (EPI). This mark aids in determining the validity of the host image and identifying ownership disputes [3]. The

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watermarking approaches are categorized according to the needs of the host image in the extraction watermark image process into blind and non-blind watermarking techniques. In the blind technique, the extraction phase is independent of the host image, whereas the non-blind technique requires the host image for extraction of the watermark. Depending on the field of work, watermarking approaches can be divided into two types. One of them is the spatial domain watermarking technique, where watermark bits are inserted into the host image by altering its pixel values. The second watermarking method is the transform domain by converting the images to the frequency domain, and the embedding is done by modifying the frequency domain coefficients of the host image. In contrast to the first, the watermarking approaches using the transform domain are more powerful due to watermark is embedded by altering the coefficients within the transformation process [4]. The transforms that are most frequently used are discrete cosine transform (DCT), discrete wavelet transform (DWT), discrete Fourier transform (DFT), and singular value decomposition (SVD). The main feature of the DCT-based watermarking technique is it outperforms others due to its resistance to image compression attacks [2]. Regarding the growing demand from mobile radio users for multimedia services, higher data rates, increased bandwidth availability, and the expected increase in Internet of Things (IoT) related data traffic, the emerged of fifthgeneration (5G) and Beyond 5G (B5G) wireless communication systems to address raised demands that exceed the capabilities of earlier generations of wireless networks. Non-orthogonal multiple access (NOMA) scheme has been regarded as revolutionary, capable of achieving higher spectrum efficiency and supporting a wider connection than common orthogonal multiple access approaches [5]. 5G networks rely mainly on universal filtered multicarrier (UFMC) multicarrier modulation techniques to transmit data, which minimizes peakto-average power ratio (PAPR) and bit error rate (BER) for input data when compared with traditional wireless multicarrier modulation [6]. Polar codes are the most efficient error correction codes (ECC) techniques. Polar codes are presently employed in 5G networks and are prime candidates for B5G. The symmetry in encoding and decoding algorithms of polar code plays an important role. In addition to ECC, the modulation and multiple access schemes form the physical layer essentials [7]. To protect the transmitted data in public channels, chaotic encryption is used. Chaotic systems have distinct and desirable properties, like high sensitivity to initial conditions and control parameters [8].

This work offers the design of a watermarking algorithm to protect medical images from numerous tamperings that occur during data traffic in wireless networks by employing polar code, UFMC modulation, and DCT with the help of the NOMA scheme for multiusers over Rayleigh and Gaussian noise channels. The proposed algorithm presents simultaneously low BER, low execution time, high imperceptibility, robustness, and security levels for watermarked images that satisfy 5G requirements. This paper is structured as follows: The following section contains a list of related works. The primary focus of the proposed work is found in Section 3. Preliminaries used in the proposed scheme are given in Section 4. The significant metrics utilized in Section 5. The proposed approach is provided in Section 6, while the explanation and experimental results are provided in Section 7. In Section 8, comparisons with earlier studies are provided. In Section 9, the paper's conclusions are presented.

2. Related work

Many studies on image watermarking techniques have been performed. The authors in [9] present a hybrid dual watermarking (image and text) technique for healthcare setups. Dual watermarks are embedded into a radiological image utilizing a DWT-SVD based on a watermarking approach. Hamming, BCH, Reed–Solomon (RS), and hybrid ECC are applied to improve the robustness of the watermark medical image. The experimental findings of the suggested method are Peak Signal to Noise Ratio (PSNR) = 37.87 and Normalized Cross-Correlation (NCC) 0.8994 at gain factor =0.05 for hybrid model and tested under different attack types. The limitations of this algorithm are the encryption process and execution time, which are not being considered.

In [10], the authors presented a selective DWT supported by a spread-spectrum watermarking algorithm for embedding medical image. The DWT coefficient is selected for the embedding phase using a threshold of the coefficient values in the column. The host and watermark images have been embedded in selection coefficients for the first- and second-level DWTs, respectively. BCH was applied before embedding to enhance the robustness. The findings are PSNR =37.75 and NCC= 0.6148 at a gain factor of 0.5, and they were also tested under various attack types. The limitations of this method are low PSNR and NCC, and the execution time is not considered.

The authors in [11] suggested a blind medical image watermarking algorithm based on Fast Discrete Curvelet Transform (FDCuT) and DCT. FDCuT is employed on a medical image to obtain

various frequency coefficients of its curvelet decomposition. The high frequency coefficients of FDCuT are applied to DCT, while mid-band frequency coefficients are modified by Gaussian Noise. The simulation results are PSNR = 55.06 and NCC = 0.9230 at a gain factor of 2, execution time = 29.95, and were tested under various geometric attacks. The fact that this method employs no security measures is one of its limitations, as well as the high processing time.

The authors in [12] produced an approach for multiple watermarking based on DWT, DCT and SVD for healthcare setups. For identification issues, the suggested approach utilizes three medical watermarks in the form of a Lump image, the doctor's signature and the diagnostic information of the patient. The robustness is improved by using a back propagation neural network on the extracted image to minimize the effects of noise. Also, the security is increased by applying Arnold transform prior to embedding process into the host image. Further, doctor signature and diagnostic information watermark images are also encoded by Hamming code and arithmetic encoding technique, respectively. The simulation results illustrate that the suggested approach has PSNR= 43.88 and NCC= 0.9547 at a gain factor of 0.01, and it is also tested under different attacks. The limitation of this method is that execution time is not considered.

In [13], the authors presented a combined DCT and successive division based on host and watermark image schemes, respectively. The findings are PSNR = 51.6464 and NCC= 0.9997, and they were also tested under cropping attack only; the proposed method has good imperceptibility and a low execution time of 0.463. This technique's drawback is that it doesn't employ any security features.

The researchers in [14] present an image watermarking algorithm by applying block-based DCT coefficient alteration. The difference between the DCT coefficients of the two blocks is determined and modified depending on the watermark bit to bring it within a preset range. The suggested method has a PSNR of 41.66 and was tested under different attacks, but the execution time is not considered.

The authors in [15] introduced a medical image watermarking method by combining DWT and SVD to protect the image exchange via telemedicine and avoid any confusion between patient data. The experimental results of the suggested scheme are PSNR = 57.04, SSIM = 0.9998, and MSE = 0.1251. In addition, it has been tested under different attacks and has good robustness, but the execution time and BER are not considered.

The researchers in [16] present an image watermarking scheme that utilizes DWT-SVD in the Fractional Order Fourier Transform (FRFT). The experimental evaluation of PSNR = 57.31 and SSIM = 0.87 under no attacks, whereas the limitation of this method did not consider the execution time and encryption process.

In [17], the authors suggested an image watermarking scheme by embedding a stego-text into the least significant bit (LSB) of the DCT coefficient by utilizing a linear modulation algorithm. The findings are PSNR = 43.30, NCC = 1, and SSIM = 0.9937 under no attacks, whereas the limitation of this scheme did not consider the execution time and use of security features.

The previously stated approaches lack crucial features required to make a balanced tradeoff in the performance of the watermarking algorithm, including imperceptibility, robustness, security, BER, and processing time for the embedding and extraction processes. In order to fulfill all the mentioned requirements, a secure image watermarking technology is proposed that provides high imperceptibility and robustness against attacks. Also, very low processing time, compatibility with high-speed networks, low BER, and better privacy for patients' identities.

3. Research contributions

The contributions of this research are as follows: I. High imperceptibility, robustness, and security were obtained for the proposed watermarking algorithm compatible with 5G networks used in telemedicine and telediagnosis applications.

II. The polar code achieves additional robustness for sensitive data and improves BER performance.

III. A novel, efficient, simple image watermarking based on DCT for multiusers is developed using data normalization to overcome high computation costs, processing time problems, and signal recovery quality.

IV. The proposed approach is robust against geometric attacks.

4. Preliminary

4.1 NOMA scheme

NOMA has evolved a significant approach for 5G wireless networks due to massive connectivity and high data rate. NOMA scheme can be performed power-domain (PD), code-domain (CD) or multiple domains. The superposition coding (SC) principle is used in PD-NOMA to transmit data of numerous



Figure. 1 Two-user downlink system of the NOMA scheme [18]



Figure. 2 Block diagram of the general UFMC scheme [20]

users using a single time-frequency resource. The downlink multiuser is identified by assigning different power at the transmitter, and a successive interference cancellation (SIC) method is used at the receiver side for decoding data from distinct users. As shown in Fig. 1, the downlink PD-NOMA case in the base station (BS) with two users is regarded, where U_1 and U_2 are near user and far user, respectively. SC is done at the BS to transmit data with different power is represented as:

$$s = \sqrt{P_1}s_1 + \sqrt{P_2}s_2$$

= $\sqrt{\alpha P}s_1 + \sqrt{(1-\alpha)P}s_2$ (1)

By assuming that the total power, denoted as P, is normalized to unit energy for analysis simplicity. The power allocation factor (PAF) is represented by α with P₁= α P and P₂ = (1 - α) P. The symbols s₁ and s₂ represent the transmitted signals from the BS to U₁ and U₂, respectively. The received signal at U_{θ} can be described as follows:

$$r_{\theta} = h_{\theta} \cdot s + v_{\theta}, \ \theta = 1,2 \tag{2}$$

where h_{θ} and v_{θ} represents the channel response, when $|h_1|^2 > |h_2|^2$, indicating that the channel condition for the near user (U₁) is stronger than that for the far user (U₂). As a result, the stronger user gets less transmit power, while the weaker user gets more. On the user end, the signal U₂ is initially decoded by treating the signal U₁ as interference because it has a larger share of transmit power. The signal U₁ can then be decoded by conducting SIC to remove U₂ from received signal, as follows:

$$r_{1} = h_{1} \cdot s + v_{1} - h_{1} \sqrt{P_{2}} \hat{s}_{2}$$

= $h_{1} \cdot \left(\sqrt{P_{1}} s_{1} + \sqrt{P_{2}} s_{2}\right) + v_{1} - h_{1} \sqrt{P_{2}} \hat{s}_{2}$ (3)

where \hat{s}_2 indicates a demodulated signal of U₂ [18].

4.2 UFMC transmission scheme

UFMC is one of the candidate technologies to satisfy 5G networks. The waveform of UFMC distributes several subcarriers into sub-bands. As a result, the cyclic prefix and out-of-band emission are reduced, which improves the spectral efficiency. UFMC is a scheme that filters blocks of subcarriers before their being transmitted and received to eliminate inter-carrier and inter-symbol interferences. UFMC stands modulation as а technique encompassing attributes of both a generalized filter bank multicarrier technique (FBMC) and filtered OFDM. Within the UFMC system, there exists a straightforward adaptability to customize the subband width and filter length, thereby aligning with the precise demands of individual users [19].

As shown in Fig. 2, a multicarrier system with N total number of subcarriers is partitioned into B subbands, with each subband including many successive subcarriers, i.e., each subband contains K = N/B subcarriers. In theoretical terms, the number of carriers in the *i*th subband is K_i , for i = 1, 2,.., B. In fact, for purposes of simplicity, normally divides each sub-band equally. Foremost, specific *Vol.17, No.3, 2024* DOI: 10.22266/ijies2024.0630.06



Figure. 3 Polar code encoding: N = 8, k = 4, F = [1,2,3,5], uF = (0,0,0,0) and uFc = (1,0,0,1). The result codeword is x = (0,0,0,0,1,1,1,1) [21]

information bits are mapped to symbols using M-QAM. These symbols are allocated to each subband using average carrier allocation. For the i^{th} subband, the symbols allocated in the frequency range are Si and their length is K_i . Then, these symbols are converted into time domain signals S_i via N-point inverse fast Fourier transform (IFFT). Notice how IFFT differs from traditional transformations here. According to the IFFT module, the time domain signal S_i of the i^{th} subband can be represented as:

$$s_i(l) = \frac{1}{\sqrt{N}} \sum_k S_i(k) e^{\frac{i2\pi kl}{N}}$$

$$l = 0, 1, \dots, N - 1$$
(4)

After that, each subband is filtered. The discrete time signal is created by adding signals from filtered subbands. As a result, the superposition of all subband symbols, i.e. the transmitted signal x, may be described as:

$$x(l) = \sum_{i=1}^{B} s_i(l) * f_i(l)$$

$$l = 0, 1, \dots, L + N - 2$$
(5)

Where * indicates convolution operation, $S_i(l)$ is a signal in time domain, $f_i(l)$ is impulse response of the FIR filter and L represents the length of the filter [20].

4.3 Polar code

Arikan first introduced the polar code in 2009. It is generally a new type of error-correcting linear block code. Polar codes are based on the phenomena of channel polarisation, which is an important factor in reaching Shannon's capacity. Channel polarisation is strategy of spreading channel capabilities across distinct instances, or more accurately uses, of a communication channel while preserving entire capacity.

Polar codes generate a range of good and bad channels, allowing data bits to be sent across the good channels whereas the entry to the bad channels is frozen. Let the input vector $u = [u_1, u_2, ..., u_N]$, a polar code encodes k data bits into N coded bits using (N - k) redundant bits, which are often known as

'frozen bits. Polar code is usually defined by the parameters (N, k, F, uF), where $F \in \{1, 2, ..., N\}$ indicates the position of frozen bits, while uF is (N - k) bits of frozen bits, which are well-known at the decoder , therefore, these parameters determine its performance.. For any encoder G_N , the polar encoding process can be characterised as follows:

$$x = uG_N \tag{6}$$

Where G_N is the n^{th} Kronecker product of the (2×2) kernel matrix, which represents the encoding transformation G_2 . More precisely, Arikan's kernel G_2 may be described in matrix notation as:

$$G_2 = \begin{bmatrix} 1 & 0\\ 1 & 1 \end{bmatrix} \tag{7}$$

while the *N*-bit encoder G_N is described as:

$$G_{N} = G_{2}^{\otimes n} = \begin{bmatrix} G_{N/2} & 0\\ G_{N/2} & G_{N/2} \end{bmatrix}$$
(8)

As a result, Arikan's polar code has a recursive configuration that invokes $n = log_2 N$ layers of polarization, with each layer employing N/2 XOR gates. For instance, consider the following 8-bit polar code: k = 4, F = [1, 2, 3, 5], uF = (0,0,0,0), and a data bit sequence $u_{Fc} = (1,0,0,1)$. The encoded output can then be calculated using the formula below:

Fc indicates the complementary set of F, which determines the position of data bits. The codeword of

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Eq. (9) can also be obtained straight from the encoding circuit, as shown in Fig. 3. The encoding mechanism of Eq. (6) may be rephrased as:

$$x = u_{FC}G_N(FC) + u_FG_N(F) \tag{10}$$

where $G_N(F)$ is a sub-matrix of G_N having only the rows with indices in F. The polar decoder is based on successive cancellation algorithms [21].

4.4 Discrete cosine transform (DCT)

DCT is an interesting transformation technique that converts data from spatial (time) to frequency domain. DCT was substantially used for image processing challenges due to its energy compaction feature. The majority of the energy is centred at lower frequencies, then the coefficients of higher frequencies can be eliminated without causing too much data quality degradation. The DCT and its inverse can be expressed in the following mathematical formula:

$$C(u,v) = \frac{2}{\sqrt{mn}} \alpha(u) \alpha(v) \sum_{\substack{x=0\\y=0}}^{m-1} \sum_{y=0}^{n-1} f(x,y) \\ \times \cos\frac{(2x+1)u\pi}{2m} \times \cos\frac{(2y+1)v\pi}{2n}$$
(11)

$$f_{i}(x,y) = \frac{2}{\sqrt{mn}} \sum_{u=0}^{m-1} \sum_{v=0}^{n-1} \alpha(u)\alpha(v)f(x,y) \\ \times \cos\frac{(2x+1)u\pi}{2m} \times \cos\frac{(2y+1)v\pi}{2n}$$
(12)

where f(x,y) indicates the pixel value in the time domain, C(u,v) is the DCT coefficient, m and n denote the block size, and

$$\alpha(u), \alpha(v) = \begin{cases} 1/\sqrt{2} \ if \ u, v = 0 \\ 1 \ else \end{cases}$$
(13)

When substituting u = v = 0 into Eq. (11) will be obtained the DC coefficient value and all other coefficients are referred to as the AC coefficients [22].

4.5 Watermark encryption

The security of the watermark image is critical if the watermark is to survive against unauthorized access. In general, robust watermarking is insufficient to protect sensitive information from various attacks, when the embedding algorithm is broken down in any way by an unauthorized person, the information is destroyed. The encryption approach guarantees that no one can access to confidential information without providing the key employed in the encryption procedure. Chaos encryption proves to be the most suitable encryption method to protect secret data and ensure data security. Chaos mapping has characteristics such as irreversibility, pseudo-randomness, and dynamic behaviour. One of the most often utilized chaotic maps in image encryption is the Baker map. A 2-D Baker map equation is as follows:

$$\begin{aligned} & (x_{n+1}, y_{n+1}) = \\ & \left\{ \begin{pmatrix} x_n \\ p \end{pmatrix}, py_n \end{pmatrix} , \quad 0 < x \le p \\ & \left\{ \frac{(x_n - p)}{(1 - p)}, (1 - p)y_n + 1 - p , p < x \le 1 \right\}$$
(14)

where *p* is the system parameter; x_n and y_n indicate the state variables. A Baker map can produce two chaotic sequences [23]. Also, another simple and efficient chaotic map is named the logistic map and can be represented by the following equation:

$$X_{n+1} = rX_n(1 - X_n)$$
(15)

The parameter r takes a value in the range $3.57 \le r \le 4$ and x_n represents the state variables [24].

4.6 Image normalisation

There are numerous pre-processing techniques available to normalize medical images before image analysis. The process of changing the range of pixel intensity values in an image is known as image normalization. The simplest form of normalization is linear normalization, which simply divides each pixel value by the maximum value that a pixel may take. If an image is 8-bit, for instance, each pixel value will be in the range [0, 255]. Linear normalization would divide each pixel value by 255, resulting in a pixel value range of [0, 1]. Some of the advantages of image normalization include: reducing image noise and increasing image processing [25].

5. Imperceptibility and robustness analysis

Imperceptibility is an important metric that indicates the variations of the quality between a host image prior to and after the embedding process. The values of components such as NCC, SSIM, and PSNR are commonly used to calculate imperceptibility.

NCC test is used to examine the relationship between the host image and the extracted watermark. Let a watermark (W_1) of size N × N, then NCC can be calculated as:



Figure. 4 Block diagram of image watermarking with embedding and extraction processes of the proposed Normalized DCT and Polar-coded UFMC Assisted NOMA scheme per user

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$$NCC = \frac{\sum_{i=1}^{N} \sum_{j=1}^{N} W_1(i,i) \times W_1^{*}(i,j)}{\sum_{i=1}^{N} \sum_{j=1}^{N} [W_1(i,i)]^2}$$
(16)

Where W_1 and W_1^* are original and extracted watermark images, respectively. The SSIM index is used to determine the degree of similarity between the host image (W₂) and its watermarked version (W₃), SSIM can be described as:

$$SSIM = l(W_3, W_2)c(W_3, W_2) \ s(W_3, W_2)$$
(17)

Where $l(W_3, W_2)$, $c(W_3, W_2)$, and $s(W_3, W_2)$ are comparison functions of luminance, contrast, and structure, respectively. While, for an image with dimensions of M × M, M=512, the PSNR is defined as:

$$PSNR = 10 \log_{10} \frac{M \times M \times max[W_2(i,j)]^2}{\sum_{i=1}^{M} \sum_{j=1}^{M} [W_2(i,i) - W_3(i,i)]^2} \quad (18)$$

In addition, the mean square error (MSE) between the host image and the watermarked image W_3 is expressed as:

$$MSE = \sum_{i=1}^{M} \sum_{j=1}^{M} [W_2(i,i) - W_3(i,i)]^2 \quad (19)$$

Both SSIM and NCC have values ranging from 0 to 1. Furthermore, a higher SSIM value indicates better watermark invisibility, while a higher NCC value indicates stronger robustness. A high PSNR value is preferred since it implies that there is a tiny difference between the host and the watermarked image. Several geometric attacks try to erase or hide a watermark image from a host image in order to test the scheme's robustness [26]. The main attack types used in this work are average filter, rotation, crop, histogram equalization, gaussian noise, and median filter.

6. Proposed watermarking algorithm

This part provides a detailed description of the suggested watermarking technique for secure medical image exchange. The block diagram of the proposed watermarking technique is shown in Fig. 4, which includes normalized DCT and Polar-coded UFMC Assisted NOMA scheme, which are implemented to create a new imperceptible, robust and simple watermarking technique to fulfill copyright protection. The proposed approach works well satisfies and the requirements for imperceptibility, security, and robustness of different attacks; therefore, it is appropriate for medical images exchanged in telemedicine applications.

6.1 Watermark embedding algorithm

The watermark image (W_1) used in this scheme is a 64×64 embedded in a 512×512 host image (W_2) . The steps of the proposed embedding process are as follows:

Step 1: The host and watermark images should be converted to grayscale images.

Step 2: Apply 16-bit analogue to digital converter (ADC) to the watermark image.

Step 3: Reshape the sequence of the Baker map to a 64×64 matrix and apply 16-bit ADC.

Step 4: Perform XOR operation between Step 2 and Step 3

Step 5: Convert bits in **Step 4** to decimals using a 16bit digital-to-analogue converter (DAC).

Step 6: Apply the DCT host image.

Step 7: Normalize the watermark image and apply the DCT.

Step 8: Divide the host image into 8×8 square blocks. **Step 9**: W₁ is inserted into W₂ as follows:

Watermarked image $(W_3) = W_1 + a \times W_2$, a: Watermark embedding intensity

Step 10: Apply IDCT to the watermarked image.

Step 11: Convert the normalized value of the watermark image to binary using 16-bit ADC.

Step 12: Convert the chaotic sequence of the Logistic map to 16 bits/ sample.

Step 13: Apply XOR between Step 11 and Step 12.

Step 14: Use frozen bits of the polar encoder from **Step 13** after padding.

Step 15: Apply 16-QAM modulator.

Step 16: Reshape data into 16 subbands and each of 16 subcarriers to perform the UFMC modulation scheme.

Step 17: Apply PAF for each user to achieve the NOMA scheme; for user 1, PAF=0.25, and user 2, PAF=0.75.

6.2 Watermark Extraction Algorithm

The received watermarked image (W₃) of size 512×512 can be extracted in the following steps:

Step 1: Appling SIC to decode data for the specified user.

Step 2: Reshape data into 16 subbands and each of 16 subcarriers to perform the UFMC demodulation scheme.

Step 3: Apply 16-QAM demodulator.

Step 4: Apply successive cancellation decoder, location of frozen bits, known to the decoder.

Step 5: Select frozen bits of the polar decoder from **Step 4** after removing zero padding.

Step 6: Convert the chaotic sequence of the Logistic map to 16 bits/ sample.

Step 7: Perform XOR between **Step 5** and **Step 6**. **Step 8**: Convert bits in Step 7 to decimals using a 16-bit DAC.

Step 9: Convert bits in **Step 4** to a decimal using 16bit DAC.

Step 10: Multiplying Step 9 by Step 8.

Step 11: Apply DCT.

Step 12: Extract the watermark as follows:

$$W_2 = \frac{W_3 - W_1}{a}$$

Step 13: Apply IDCT.

Step 14: Apply 16-bit ADC to the extracted watermark.

Step 15: Apply 16-bit ADC to the Baker map.

Step 16: Perform XOR between Step 1 and Step 15. Step 17: Apply 16-bit DAC to Step 16.

7. Simulation results

This section analyses the proposed watermarking technique evaluation by measuring watermark imperceptibility and robustness. MedPix® was used to take a variety of medical images for analysis. With Matlab R2020 software running in Windows 10 and an Intel(R) Core (TM) i7-7500U laptop with 2.70 GHz 2.9 GHz, 8 GB RAM, and a 64-bit operating system, the suggested scheme was implemented. The proposed watermarking technique was tested under numerous medical images with and without various attacks. Table 1 parameter values used through simulation.

Scheme	Parameter	Value
	Total Number of subcarriers(N)	256
	Number of sub-band (B)	16
	Number of subcarriers per sub-band (K)	16
UFMC	Filter type	Dolph Chebyshev
	Side Lobe Attenuation	40 dB
	Modulation scheme	16-QAM
	Number of bits per subcarrier	4
	Number of users	2
NOMA	Power allocation factor (PAF)	0.25
	Channel Fading	Rayleigh- Flat
D 1	Length of polar code (N)	32 bits
Polar	Number of information (k)	12 bits
coue	Number of frozen (N-k)	20 bits
ADC	Bits/sample	16

Table 1. parameters for simulations

7.1 Imperceptibility test

NCC, SSIM, PSNR, and MSE metrics have been used to evaluate the imperceptibility of the watermarked image yielded by the suggested scheme. Fig. 5 shows the host, watermark, and watermarked images with their corresponding watermarks extracted from them. Table 2 presents the objective metrics of watermarked images acquired by the suggested technique for two users.

It is evident from the findings above that the watermarked image's average PSNR value is higher than 68 dB, and NCC with approximately unity value has been obtained. In addition, the extracted image cannot be decrypted if the receiver knows the embedding algorithm unless it has a decryption secret key. Therefore, it is clear that high imperceptibility is preserved for watermarked images, and thus, the scheme can be applied in many medical image exchanges.

7.2 Robustness test

Watermarked images are subjected to different attacks to evaluate the proposed algorithm's resilience.

The robustness of the approach is thought to be high for that attack if the retrieved watermark is reasonably identifiable. The outcomes of multiple attacks on the watermarked image in terms of PSNR and NCC are shown in Fig. 6. The findings shown in Fig. 6 make it evident that the suggested scheme has strong resilience and can effectively defend against all of the attacks indicated.

7.3 Processing time analysis

The processing time of this scheme depends on the size of the host image and the watermark used.

The larger the image dimensions, the longer the processing time. In addition, the total processing time of the watermark processing is measured as the sum of the respective times required for the embedding and extraction processing. The processing time evaluation of the proposed method is shown in Table 3.

7.4 Performance analysis

The proposed scheme uses polar code within the embedding algorithm and as ECC to enhance the system performance in terms of BER. The BER metric measures the amount of incorrect bits that were retrieved from the received image through the wireless channel. A lower BER indicates the effectiveness of the transmission system and

	Name	Host Image	Watermark Image	Watermarked Image	Extracted Encrypted watermark	Extracted Decrypted watermark
•1	Brain					
	Chest	Pulmonary Angio, AP View 40"	则⋛	Putracray Anjor AP View 40"	Engeneration (Construction) Construction (Construction) Co	则
Use	Hand		则♪		alan Ar Ang Ar Ang Ar Ang Ar	
	Knee	Gr.		and a second sec		
User 2	Brain		Copy Rights Reserved			Copy Rights Reserved
	Chest	Support Village	Copy Rights Reserved			Copy Rights Reserved
	Hand		Copy Rights Reserved			Copy ∟ Rights Reserved
	Knee		Copy Rights Reserved			Copy Rights Reserved

Figure. 5 watermarked and extracted images without attacks

Attacks typeWatermarked imageExtracted watermarkWatermarked imageExtracted watermarkaverage filtering using 3×3 pixels neighborhoodImageImageImageImagePSNR=50.0199NCC=0.9835PSNR=48.9777NCC=0.9896rotation with 30- anticlockwiseImageImageImageImagePSNR=30.0199NCC=0.9835PSNR=48.9777NCC=0.9896rotation with 30- anticlockwiseImageImageImageImagePSNR=33.9435NCC=0.9832PSNR=3.2363NCC=0.9855Guussian noise with zero mean and 0.01 varianceImageImageImageImagePSNR=29.273NCC=0.94711PSNR=28.8201NCC=0.9428Cropping one-fourth from the left sideImageImageImageImagePSNR=20.5427NCC=0.9775PSNR=20.2471NCC=0.9698histogram equalizationImageImageImageImagePSNR=11.3219NCC=0.9537PSNR=11.229NCC=0.9529median filtering using 3 × 3 pixels neighborhoodImageImageImagePSNR=36.2816NCC=0.9745PSNR=36.1742NCC=0.9749JPLG compression with a quality factor of 50ImageImageImagePSNR=48.3865NCC=0.9754PSNR=48.2637NCC=0.9767		Use	er 1	User 2			
imagewatermarkimagewatermarkaverage filtering using 3 × 3 pixels neighborhoodImageImageCopy Rights ReservedPSNR- 50.0199NCC-0.9835PSNR-48.9777NCC-0.9896rotation with 30- anticlockwiseImageImageImageImagePSNR-33.9435NCC-0.9832PSNR-33.2363NCC-0.9855Gaussian noise with zero mean and 0.01 varianceImageImageImageImagePSNR-29.273NCC-0.9471PSNR-28.201NCC-0.9428Cropping one-fourth from the left sideImageImageImageImagePSNR-20.5427NCC-0.9775PSNR-28.201NCC-0.9698histogram equalizationImageImageImageImagePSNR-11.3219NCC-0.9537PSNR-11.2239NCC-0.9698ImagePSNR-36.2816NCC-0.9745PSNR-36.1742NCC-0.9529PEG compression with a quality factor of 50ImageImageImageImagePSNR-48.3865NCC-0.9754PSNR-48.2637NCC-0.9767	Attacks type	Watermarked	Extracted	Watermarked	Extracted		
PSNR= 50.0199NCC= 0.9835PSNR= 48.9777NCC= 0.9896rotation with 30- anticlockwiseImage: Second Sec	average filtering using 3× 3 pixels neighborhood	image	watermark	image	Copy Rights Reserved		
rotation with 30- anticlockwiseImage: Second Secon		PSNR= 50.0199	NCC= 0.9835	PSNR= 48.9777	NCC= 0.9896		
PSNR=33.9435NCC= 0.9832PSNR=33.2363NCC= 0.9855Gaussian noise with zero mean and 0.01 varianceImage: Second Sec	rotation with 30° anticlockwise	8			Copy Rights Reserved		
Gaussian noise with zero mean and 0.01 varianceImage: Serie definition PSNR= 29.273Image: Serie definition PSNR= 28.8201Image: Serie definition PSNR= 28.8201Image: Serie definition PSNR= 28.8201Image: Serie definition ReservedCropping one-fourth from the left sideImage: Serie definition PSNR= 20.5427Image: Serie definition PSNR= 20.5427Image: Serie definition PSNR= 20.2471Image: Serie definition PSNR= 20.2471Image: Serie definition Reservedhistogram equalizationImage: Serie definition PSNR=11.3219Image: Serie definition PSNR= 11.2239Image: Serie definition PSNR= 11.2239Image: Serie definition PSNR= 11.2239Image: Serie definition 		PSNR=33.9435	NCC= 0.9832	PSNR=33.2363	NCC= 0.9855		
PSNR= 29.273NCC= 0.9471PSNR= 28.8201NCC= 0.9428Cropping one-fourth from the left sideImage: Signal state s	Gaussian noise with zero mean and 0.01 variance	a de la dela dela dela dela dela dela de			Copy Rights Reserved		
Cropping one-fourth from the left sideImage: Side Side Side Side Side Side Side Side		PSNR=29.273	NCC= 0.9471	PSNR= 28.8201	NCC= 0.9428		
PSNR= 20.5427NCC= 0.9775PSNR= 20.2471NCC= 0.9698histogram equalizationImage: Stress of the stress of	Cropping one-fourth from the left side	e e			Copy Rights Reserved		
histogram equalizationImage: Simple segmet and segme		PSNR= 20.5427	NCC= 0.9775	PSNR= 20.2471	NCC= 0.9698		
PSNR=11.3219NCC= 0.9537PSNR= 11.2239NCC= 0.9529median filtering using 3 × 3 pixels neighborhoodImage: Second S	histogram equalization	ł		*	Copy Rights Reserved		
median filtering using 3 × 3 pixels neighborhoodImage: Second se		PSNR=11.3219	NCC= 0.9537	PSNR= 11.2239	NCC= 0.9529		
PSNR= 36.2816NCC=0.9745PSNR= 36.1742NCC=0.9749JPEG compression with a quality factor of 50Image: Second	median filtering using 3 × 3 pixels neighborhood	ł			Copy Rights Reserved		
JPEG compression with a quality factor of 50Image: Second		PSNR= 36.2816	NCC=0.9745	PSNR= 36.1742	NCC=0.9749		
PSNR= 48.3865 NCC=0.9754 PSNR=48.2637 NCC=0.9767	JPEG compression with a quality factor of 50	a b			Copy Rights Reserved		
		PSNR=48.3865	NCC=0.9754	PSNR=48.2637	NCC=0.9767		

Figure. 6 Watermarked and extracted watermark imaged against various attacks

		Use	er 1		User 2				
image	NCC	SSIM	PSNR	MSE	NCC	SSIM	PSNR	MSE	
Brain	0.9997	0.9966	69.5761	0.4399	0.9908	0.9890	68.1254	0.3363	
Chest	0.9934	0.9361	69.5371	0.3864	0.9966	0.9824	68.0008	0.2905	
Hand	0.9924	0.9242	69.5425	0.3846	0.9948	0.9831	68.0119	0.3856	
Knee	0.9998	0.8876	69.5884	0.3930	0.9970	0.8946	67.9884	0.3959	

Table 2. Perceptual quality metrics of watermarked medical images under no attacks

Table 3. Processing time evaluation

Image /user	Image size	Embedding Time	Extraction Time	Total Time
Knee	28.6	0.206	0.1224	0.3284
/user 1	KB	(Sec.)	(Sec.)	(Sec.)
Knee	30.2	0.215	0.1295	0.3445
/user 2	KB	(Sec.)	(Sec.)	(Sec.)



Figure. 7 BER performance of the proposed polar coded UFMC assisted NOMA system

embedding algorithm. As shown in Fig. 7, two scenarios are investigated, the first one is a watermarking algorithm using traditional DCT with UFMC-assisted NOMA scheme for two users, whereas the second one is a watermarking algorithm using normalized DCT with polar coded UFMCassisted NOMA scheme for two users. It is clear that the proposed scheme gives a very low BER and thus reduces the channel distortion.

8. Comparative study

This section illustrates a comparison between the proposed algorithm and other popular algorithms found in the literature. Table 4 presents the database and parameters used in the past studies, while Table 5 lists the PSNR and NCC values of the extracted watermarks with and without attacks. The host image used in Table 5 is the Knee image of user 1. As observed in the table, the watermarked images produced by the suggested approach have greater PSNR values than the other works. It means that the host image suffers less distortion as a result of the watermark insertion. The images that are received may be damaged by different attacks after being transmitted over a wireless channel for each user. Thus, under attacks, the comparison will be performed in terms of NCC. The watermarked image of the proposed algorithm that is subjected to Average Filtering, Rotation, Cropping, and JPEG Compression attacks is more robust than other schemes, whereas it gives acceptable robustness when subjected to Gaussian Noise, Histogram Equalization, and Median Filtering attacks. In addition, the average total execution time for the proposed algorithm is about 0.3284 Sec. When

Reference	[9]	[10]	[11]	[12]	Proposed
Parameter					-
Host image size	512×512	512×512	1024×1024	512×512	512×512
Watermark image size	256×256	64×20, 80×25,	128×128	256×256	64×64
_		99×31			
Transform for	DWT+SVD	DWT	FDCuT+DCT	DWT+DCT+SV	Normalized
Watermark Embedding				D	DCT
Gain factor	0.01 to 0.1	1 to 5	2 to 8	0.01 to 0.2	0.01
Colorimetry	grayscale	grayscale	grayscale	grayscale	grayscale
Security mechanism	-	Spread	Gaussian	Arnold	Baker Map
		Spectrum	Noise	transform	
ECC	BCH+RS+	BCH	-	Hamming code	Polar code
	Hamming code			_	

Table 4. Database and parameters of previous works

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Reference	[9]		[10]		[11]		[12]		Proposed	
Metrics	PSNR	NCC	PSNR	NCC	PSNR	NCC	PSNR	NCC	PSNR	NCC
No Attack	37.87	0.8994	37.75	0.6148	55.06	0.9230	43.88	0.9547	69.5884	0.9998
Average Filtering	-	-	-	-	-	0.8688	-	-	50.0199	0.9835
Rotation	-	-	-	-	-	0.7895	-	-	33.9435	0.9832
Gaussian Noise	-	0.3289	-	0.7394	-	0.9322	-	0.9466	29.273	0.9471
Cropping	-	0.9481	-	-	-	0.9704	-	-	20.5427	0.9775
Histogram Equalization	-	0.8187	-	0.7402	-	0.9689	-	0.9404	11.3219	0.9537
Median Filtering	-	-	-	0.2162	-	0.9538	-	-	36.2816	0.9745
JPEG Compression	-	-	-	0.7364	-	0.7125	-	0.9787	48.3865	0.9754
Total execution time (Sec.)		-		-	29	9.95		-	0.3284	

Table 5. Robustness and processing time comparison with previous works for user 1 and Knee image

compared with other competing algorithms, it is also efficient in terms of computational time and compatible with modern high-speed communication networks.

9. Conclusions

A new approach to the watermarking technique, which uses normalized DCT and is compatible with modern communications networks for multiusers, is proposed in this work. The watermark image is encrypted employing a Baker map before embedding and then normalized, the normalized value of an encrypted image is mixed with a chaotic Logistic map, and then, the secure sequence is employed in polar code as frozen bits. The embedded medical image is transmitted using a UFMC-assisted NOMA scheme. The proposed approach is evaluated for several medical images and compared with competing schemes by various tests that were performed. It was found that PSNR is above 69 dB, and NCC is above 0.99. It has been demonstrated that the proposed watermarking technique produces better watermark imperceptibility and robustness under various attacks. Also, the minimum execution time achieved for the embedding and extracting processes is about 0.3284 Sec.. In addition, the performance analysis of the proposed method in terms of BER shows good behaviour under a wireless fading channel. Finally, the polar code is employed for many purposes, including watermarking, security, and ECC, making

the proposed scheme a promising solution for protecting the privacy of medical images.

Conflicts of Interest

The authors declare that there is no conflict of interest.

Author Contributions

Conceptualization, methodology, software, validation, formal analysis, investigation, resources, data curation, writing-original preparation, writing review, editing, and visualization have been implemented by the 1st, 2nd and 3rd authors.

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